

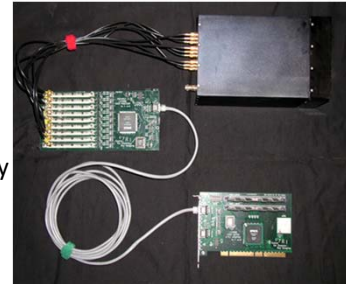
Design Of A Next-Generation Modular Gamma Camera For Small Animal Imaging

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Current Generation Modular Cameras

- Monolithic scintillation crystal
- 3x3 PMT array
- ~ 2 -2.5 mm resolution in x, y
- $> \sim 5$ mm resolution in z
- Timing (30ns)



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Motivation For New Camera

- Multi-anode photomultiplier tubes (MAPMTs) are good candidates as sensors for scintillation cameras (SPECT/PET applications)
- For small animal imaging experiments at least 10 cm x 10 cm area desired.
- Thus, tiled arrays of MAPMTs are required
- New MAPMTs may have 64 or 256 anodes per tube.
- Large number of channels that require amplification and digitization become practically not feasible. (speed, data management and power consumption)



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Objective

Design read-out electronics (*event processor*)

- that allows multiple MAPMT modules to be optically coupled to a single monolithic scintillator crystal,
- that has reduced number of readout channels,
- to be used with maximum-likelihood (ML) methods,
- that achieves precision in estimating event parameters that is close to what is achieved by retaining all signals (sufficient statistics).

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Fisher Information Matrix

- We will use FIM as the tool to quantify the information conveyed by the detector signals

$$F_{nm} = \left\langle \left[\frac{\partial}{\partial \theta_n} \ln \text{pr}(\mathbf{g}|\boldsymbol{\theta}) \right] \left[\frac{\partial}{\partial \theta_m} \ln \text{pr}(\mathbf{g}|\boldsymbol{\theta}) \right] \right\rangle_{\mathbf{g}|\boldsymbol{\theta}}$$

$\text{pr}(\mathbf{g}|\boldsymbol{\theta})$: likelihood

\mathbf{g} : set of anode signals

$\boldsymbol{\theta} = \{x, y, z, \varepsilon, t_0\}$: set of event parameters

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Cramer-Rao (CR) Lower Bound

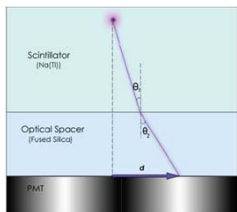
- For any covariance matrix it can be shown that

$$[\mathbf{K}_{\hat{\theta}}]_{nn} = \text{Var}\{\hat{\theta}_n\} \geq [\mathbf{F}^{-1}]_{nn}$$

- complementarity relation with the Fisher information.
- sets a lower bound on the variance of an unbiased estimator.
- In the case of position estimation, represents the best possible spatial resolution that can be achieved.

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Forward Model



Assume a gamma camera with monolithic NaI(Tl) scintillator ($n=1.85$) and fused-silica light guide ($n=1.46$), blackened entrance face blackened sides.

- Assume energy deposited at single location.
- Mean number of photoelectrons produced at the k^{th} anode;

$$\bar{n}_k(r_{int}) = \eta_k \beta_k(r_{int}) \bar{n}_{optical}$$

- Mean number of optical photons

$$\bar{n}_{optical} = \eta_{sc} \varepsilon$$

$$\eta_k \beta_k(r_{int}) \ll 1$$

- Assume number of photoelectrons in each PMT is independent and **Poisson** distributed.

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FIM of a single anode:

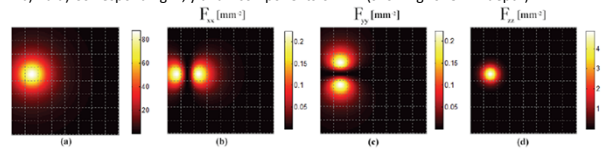
Poisson model : $\text{pr}(\mathbf{g}|\boldsymbol{\theta})$

$$F_{nm} = \sum_{k=1}^N \frac{1}{\bar{g}_k(r, \varepsilon)} \frac{\partial}{\partial \theta_n} \bar{g}_k(r, \varepsilon) \frac{\partial}{\partial \theta_m} \bar{g}_k(r, \varepsilon)$$

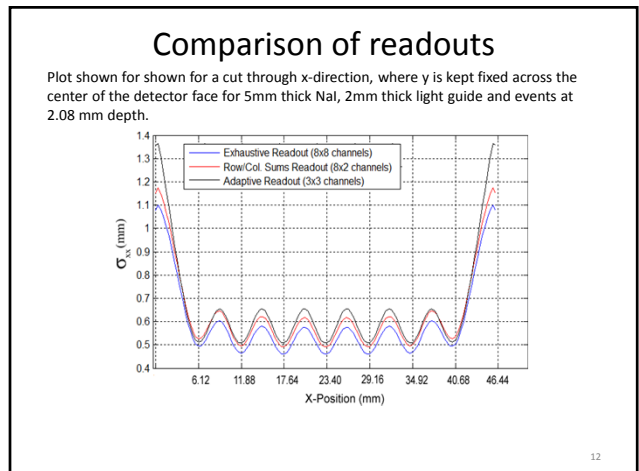
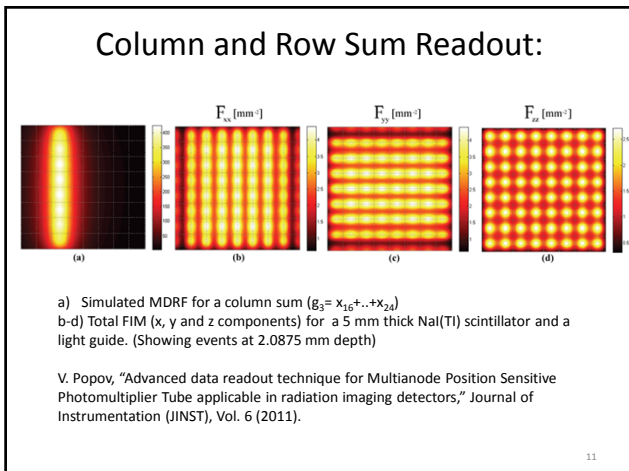
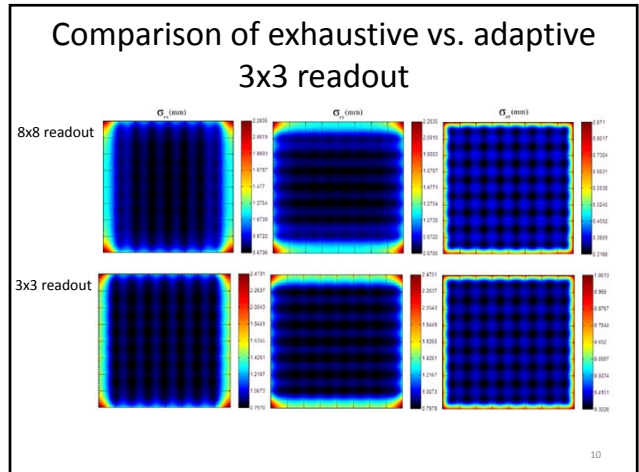
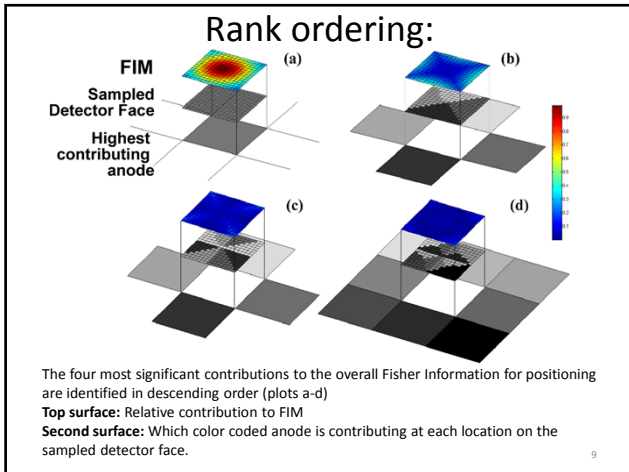
(anodes)

For example : for anode (4,2)

- a) Simulated signal
- b) b-d) Corresponding x, y and z components of FIM (showing for 3mm depth)1

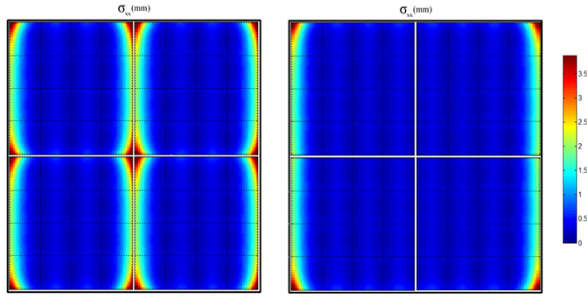


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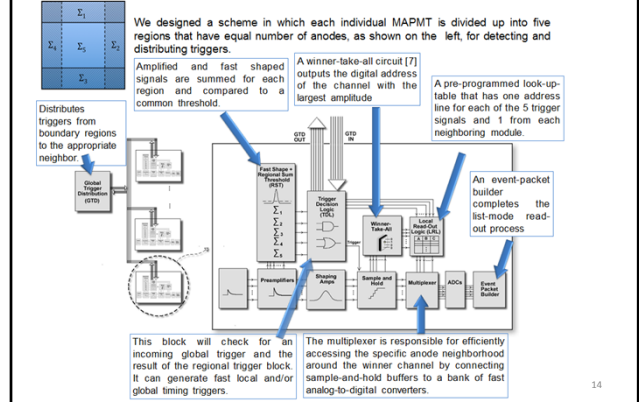


Tiling MAPMTs

- Spatial resolution decline at the edges of the individual MAPMTs
- Propose inclusion of neighboring anode signals associated for each event



Event Processor Block Diagram



Future Work

- Support precise timing/time-of-flight experiments
- Waveform sampling (can be applied to the summation of the output pulses of the constructed anode neighborhood)
- Evaluate of Domino Ring Sampling (DRS) chip - developed by Paul Scherrer Institute, Switzerland which offers digitization up to 6 GSPS sampling rates on 9 differential input channels using switched capacitor arrays (SCA)

Acknowledgements



- CGRI team