

Design, Processing, Analysis, and Reporting of Longitudinal Small-Animal SPECT Studies

inviCRO November 6, 2012



- Founded in 2008, headquartered in downtown Boston with a satellite office in Cologne, Germany
- Research team comprised of a broad range of technical disciplines including advanced degrees in: physics, optics, software engineering, electrical engineering, chemical engineering, mathematics, neuroscience, biomedical engineering and statistics.
- Three primary departments, united to execute successful contract imaging studies, advanced image analysis, and image data management
- Services
 - Full-scale image study management 12+ studies per month
 - MSAs with 7 validated partner facilities
 - Image analysis services 35,000+ scans per year
 - Broad application experience: oncology, neuroscience, toxicology, immunology, ...



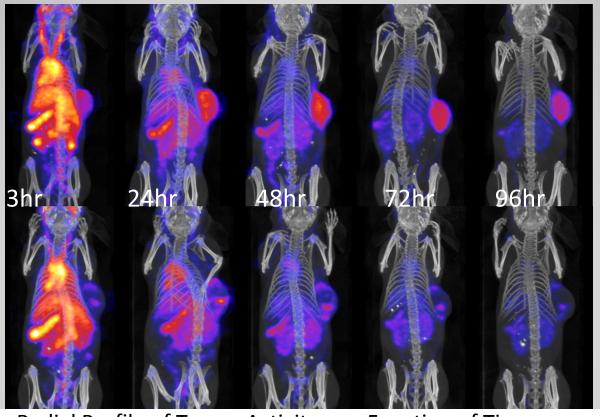
iPACS[®] and VivoQuant[™] Software

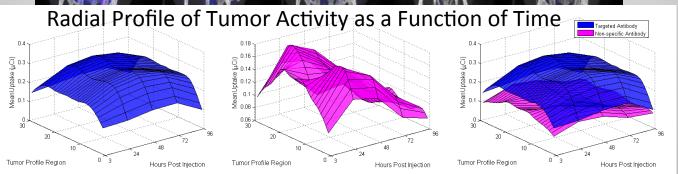
- VivoQuant™ analysis and viewing software installed at 100+ imaging labs world-wide
- iPACS® data management and archiving solution installed at 8 top pharmaceutical companies
- Developed to work with all preclinical imaging platforms and clinical DICOM data

Growth

- Supporting four clinical trials with imaging endpoints
- Advanced the iPACS® platform for GLP storage of pharmaceutical industry medical and histological imaging data
- 2013 opening of a new laboratory with multi-modal imaging, radiochemistry, and autoradiography

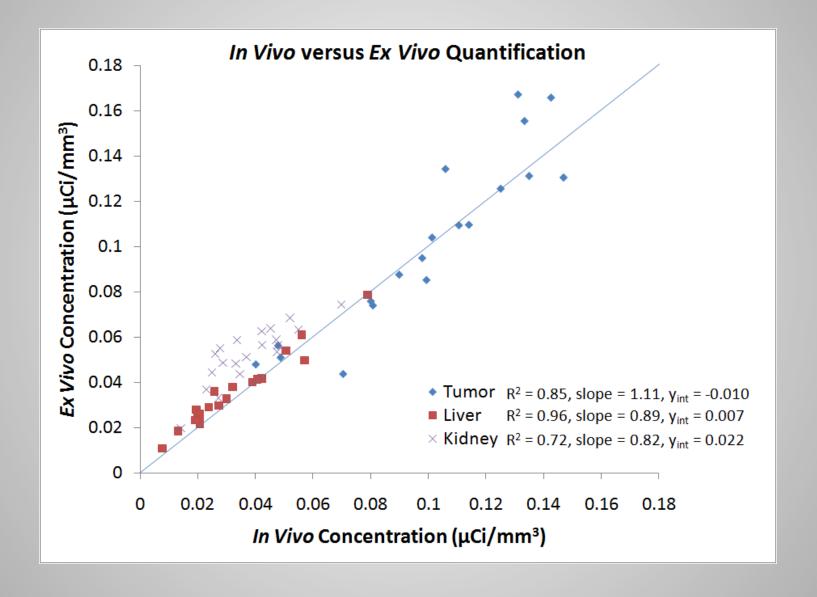






Example results from an 111In antibody tumor study. Cover of JPET, May 2011, Review on imaging antibodies in mice





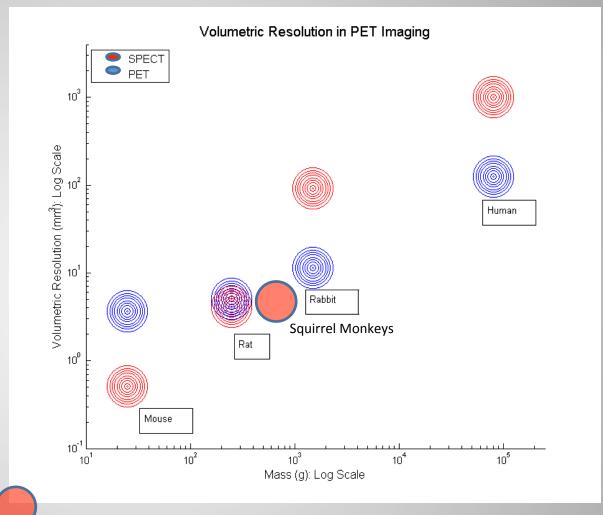
Introduction



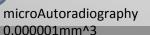
Understanding the range of sensitivities and resolutions available with *in vivo* and *ex vivo* scanning modalities

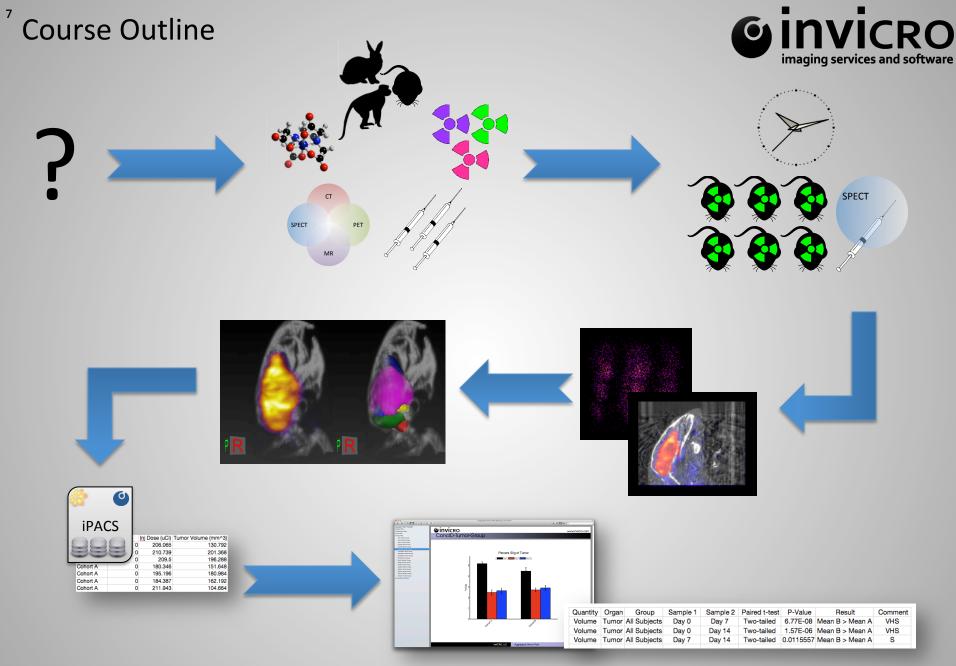
Dependencies:

- Isotope Selection
- Radiochemistry
- Pharmacokinetics
- Radiation Dosimetry
- System Manufacturer
- Acquisition Protocol



Autoradiography 0.001mm^3





Using a longitudinal SPECT/CT study to go from biological question to p < 0.01.

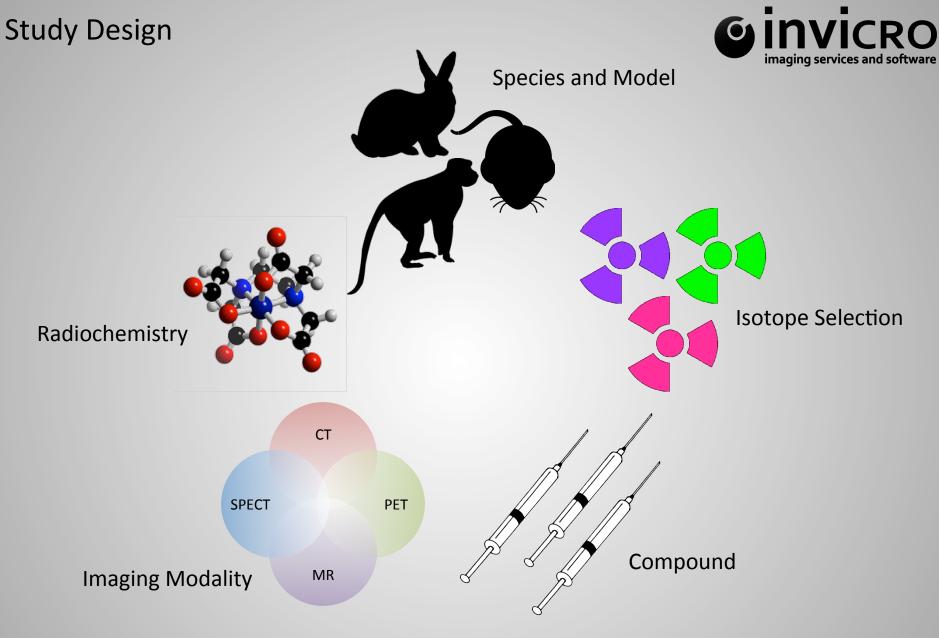




What is the biological question?

- → What are the pharmacokinetics of a liposome/protein/peptide?
- → How do the pharmacodynamics of a novel therapeutic affect the pharmacokinetics of a well-characterized radiopharmaceutical?
- → What is the tumor-to-liver ratio of a compound as a function of time?
- → What is the relationship between myocardial infarct volume and ejection fraction?
- → Is the binding affinity for a compound different between aged and young animals?
- → How do changes in mass dose impact blood clearance?

The answer is **not**: "Let's put in FDG and see where it goes."



The evaluation criteria for each of these design elements and their combination is signal-to-noise or signal-to-background ratio.

Example: How isotope selection affects signal.



Signal should be significantly* greater than background for visualization.

For an example system (NanoSPECT/CT), typical background values are in the range of 0.1-0.5 uCi/mL (depending on isotope, scan duration, and radioactivity distribution).

Therefore, assuming one isotope per molecule, the concentration of radiolabeled compound must be > 100 pM for I125 but only > 5-10 pM for I123.

Example Calculation:

Background = ~0.2 uCi/mL

Specific activity (assuming one I125 per molecule) = 2199 uCi/nmol

Let Activity Concentration = Background = 0.2 uCi/mL

Activity Concentration / Specific Activity = [0.2 uCi/mL] /[2199 uCi/nmol] = 90 pM

Thus, ~90 pM concentration of I125-labeled compound is indistinguishable from background.

^{*}Conventional wisdom states that a factor of 2.5 to 3 is deemed appropriate for signal detection tasks by human observers; there are many caveats given the context of the task.

Example: How isotope selection affects signal.



Isotope	Specific Activity (uCi/nmol)	Background (uCi/mL)	Compound Conc = Background (nM)	Compound Conc = Background (nmol/ mL)	
1251	2200	0.2	0.1	0.0001	
1231	235000	0.2	0.001	0.000001	
99mTc	520000	0.2	0.0004	0.000004	
111In	47000	0.3	0.006	0.000006	

Approximate theoretical concentration required to achieve SNR = 1. Assumes one isotope per molecule.

SPECT Isotopes	⁶⁷ Ga	123 I	125 I	¹¹¹ In	¹⁷⁷ Lu	^{99m} Tc
Half-Life (days)	3.26	0.55	59.42	2.80	6.75	0.25
Energy in keV (mean no. of gamma emissions per 100 decays)	93.2 (42.4), 184.6 (21.2), 300 (16.6)	28.0 (86.7), 159.0 (83.0)	27-32 (144.6)	171.3 (90), 245.4 (94.0)	56.7 (5.4), 112.9 (6.4), 208.4 (11.0)	140.5 (89)
Recon. Resolution (mm ³) 1mm pinh. w/Jasz	0.73	0.51	1.00	0.42	0.51	0.41
Avg. Sensitivity in 20g mouse (cps/uCi/cc, 1.0mm pinh array)	0.182	0.442	0.443	0.285	0.052	0.226
Avg. Sensitivity in 20g mouse (cps/uCi/cc, 2.0mm pinh array, ~microPET resolution)	0.73	1.77	1.77	1.14	0.21	0.90
Whole-body Absorbed Dose (Gy) per 100 μCi and a 72 hr biological half life (max dose - no biological clearance)	0.258 (0.542)	0.065 (0.077)	0.276 (5.726)	0.284 (0.556)	1.117 (3.646)	0.017 (0.019)
Specific Activity (theoretical) Ci/ µmol	40	237	2.2	47	19	522
Radioisotope/Antibody ^a	0.00375	0.005-0.008	0.01-0.3	0.02-0.16	0.01-0.1 imaging, max 2.4 therapy	0.003-0.008
Primary Labeling Method	DOTAf	direct labeling (iodination)	direct labeling (iodination)	DTPAf	DOTAf	HYNIC ^f , MAG3 ^f , hexahist-adine
Primary Strength/Use	Translatable to Ga-68 for PET	Neuro-imaging	Long half-life	Availability and Translation	Imageable and Therapeutic	Low-Priced
Primary Shortcoming	Contamination with Zn	Cost, Half-life	Long half-life	High cost	Potential Therapeutic Effect	Short half-life
Cost/mCi (\$) ^b	+++	+++	++	+++++	++	+

Example: How tissue uptake kinetics affect signal.



Tissue uptake is a function of:

- Blood flow rate = $Q(1-H)/f_{free}$
- Extravasation rate = 2PR_{cap}/R²_{Krogh} = PS/V
- Interstitial diffusion rate = Dε/R²_{Krogh}
- Binding or metabolism rate = k_{rxn}

where f_{free} = fraction of drug unbound in plasma, H = hematocrit, Q = blood flow rate (volume of blood per volume of tissue per time), P = capillary permeability, S = capillary surface area, V = tissue volume, ϵ = void fraction, D = diffusion coefficient, R_{Krogh} = capillary-to-capillary half-distance

Each of these four transport/kinetic rates may be estimated from target and compound properties to determine the rates that most/least affect uptake.

The rate-limiting step(s) will determine the meaning of "signal".

Example: How tissue uptake kinetics affect signal.



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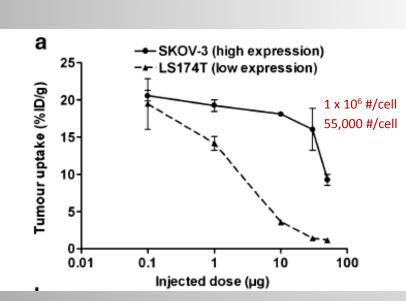
Estimations from literature values	Oxygen	18FDG	Antibody (sub- saturating)	Antibody (saturating)
Blood flow (s ⁻¹)	0.09	0.06	0.06	0.06
Extravasation (s ⁻¹)	1.4	0.003	0.00001	0.00001
Diffusion (s ⁻¹)	0.3	0.04	0.0004	0.0004
Binding/metabolism (s ⁻¹)	0.2	0.0006	0.07	0.000001

Slowest rate determines the meaning of "signal". Oxygen is a measure of blood flow, 18FDG is a measure of glucose metabolism, sub-saturating antibody a measure of extravasation/vascularity and saturating antibody a measure of antigen binding.

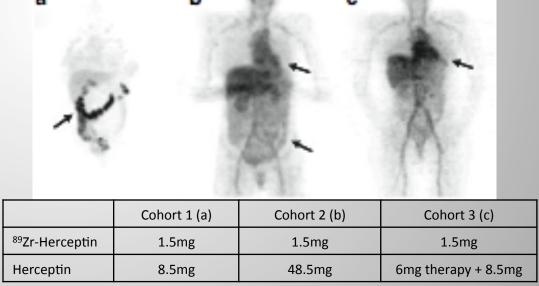
Specific Activity and Mass Dose.



- Maximum specific activity (= lowest injected mass dose) depends on:
 - Isotope
 - Isotope/ligand (labeling chemistry)
 - Can always add cold compound to lower specific activity
- Competition also factors into selection of specific activity and dose
- Specific activity determines lowest antigen expression level detectable
- Typically, lower injected mass dose is preferable, particularly for peptides and other small molecules, but not always the case.



111In-labeled anti-HER2 affibody
Tolmachev et al. 2011



Increasing Herceptin from 8.5 mg; 48.5 mg slowed blood clearance & improved tumor accumulation of ^{89}Zr -Herceptin as did 8.5 mg when the subject was on Herceptin (Dijkers, et. al. 2010)

Number of animals.



How can the study's longitudinal-ism be incorporated into statistics?

Scheibe, Nuc. Med. Bio. 35 (2008) 3-9

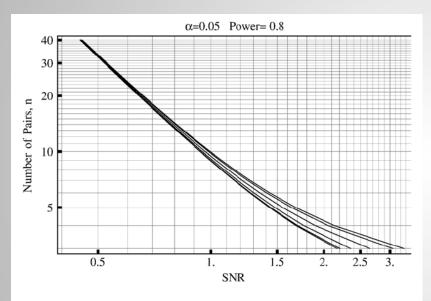
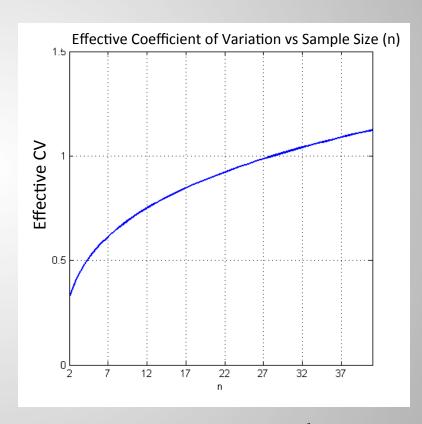


Fig. 3. Summary for two-sided test. Number of pairs (animals) required to have given size α =0.05 and power β =0.80 of two-sided Student t test using Welch's ν approximation when it is not known whether sample variances are equal. θ varies from zero to one in steps of 0.2; θ =0.0 for the rightmost curve and θ =1.0 for the leftmost curve.

SNR =
$$\frac{|\mu_1 - \mu_0|}{(\sigma_1^2 + \sigma_0^2)^{\frac{1}{2}}}$$



$$CV_{eff} = \frac{(\sigma_1^2 + \sigma_0^2)^{\frac{1}{2}}}{|\mu_1 - \mu_0|}$$

EINVICROimaging services and software

Number of animals.

How can the study's longitudinal-ism be incorporated into statistics?

Building on the work of Eckelman et. al., and Scheibe, we may use a one-way MANOVA to estimate the required effect size necessary to expect significance at a fixed significance level (alpha) and power (1-beta). Conversely, given an anticipated effect size, the number of animals required may be estimated.

$$\Delta R = \sqrt{\frac{2\delta_p}{n(\mathbf{1}^t \mathbf{D}^t \mathbf{P}^{-1} \mathbf{D} \mathbf{1})}}$$
 (1)

where ΔR is the change in the effect and n is the number of animals.

D is a scaling transformation matrix whose elements are the reciprocals of the standard deviations for each feature and **P** is a p x p population correlation matrix on the features (solved from $P = D\Sigma D^t$ where Σ is the class covariance matrix).

 δ_p is a non-centrality parameter given by $\delta_p = \frac{n}{2}(\mu_1 - \mu_2)^t \mathbf{\Sigma}^{-1}(\mu_1 - \mu_2)$ that also depends on the selection of alpha and beta.

Number of animals.

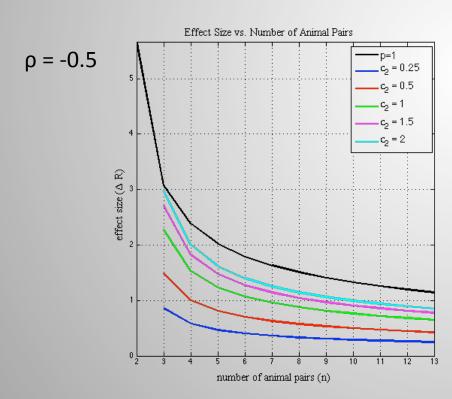


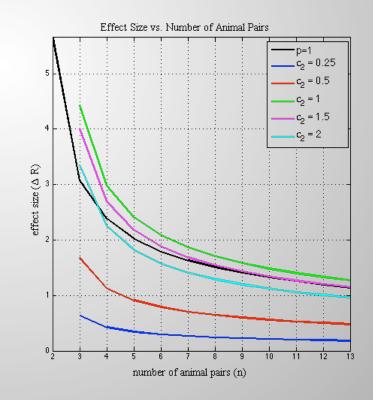
Special Case: One Feature:

$$\Delta R = \sqrt{\frac{2\sigma_1^2 \delta_1}{n}} \qquad (2)$$

Special Case: Two Features:

$$\Delta R = \sqrt{\frac{2\sigma_1^2}{n}} \left(\frac{\gamma^2 (1 - \rho^2) \delta_2}{\gamma^2 - 2\rho \gamma + 1} \right)$$
 (3)





 $\rho = 0.9$

Mathematical modeling



Mathematical modeling has widespread use in imaging and other drug development areas, focusing primarily on assessing either the pharmacokinetics (PK) or pharmacodynamics (PD) of a drug within the body.

- The pharmacokinetic phase encompasses all the events between the administration of a dose and the achievement of drug concentrations throughout the body.
- The pharmacodynamic phase encompasses all the events between the arrival of the drug at its site of action and the onset, magnitude, and duration of the biological response.

In imaging, compartmental models are typically applied to describe pharmacokinetic features like:

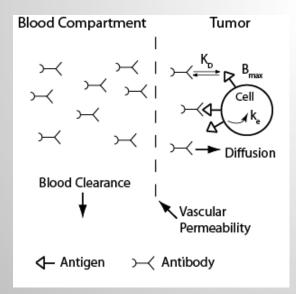
- Blood clearance (drug metabolism and excretion)
- Irreversible trapping in tissues (i.e., Patlak analysis)
- Reversible trapping in tissues (i.e., Logan analysis)

Mathematical modeling



Models, particularly compartmental models, are often used to assess image data post-acquisition (i.e., estimation of kinetic parameters). Models, especially mechanistic models, may also be used in a predictive sense.

For example, models such as this tumor model based on the Krogh cylinder model may be used to help guide preclinical study design, including parameters such as dose range and specific activity, given some criteria based on clinical need and antigen/target properties.



Baxter and Jain, Br J Cancer, 1996 Jackson et al. Br J Cancer, 1999 Thurber et al. JNM, 2007

- Krogh distributed model
 - oxygen transport in tissue (1919)
- Model assumptions
 - No convection high tumor pressure
 - Vascular tumor

Mathematical modeling



$$\frac{\partial Ab(\vec{x},t)}{\partial t} = D \cdot \nabla^2_{\vec{x},\vec{x}}(Ab(\vec{x},t)) - \frac{k_{on}}{\epsilon} \cdot Ab(\vec{x},t) \cdot Ag(\vec{x},t) - k_{off} \cdot B(\vec{x},t)$$

$$\frac{\partial B(\vec{x},t)}{\partial t} = \frac{k_{on}}{\epsilon} \cdot Ab(\vec{x},t) \cdot Ag(\vec{x},t)$$
 . $k_{off} \cdot B(\vec{x},t) - k_e \cdot B(\vec{x},t)$

$$\frac{\partial Ag(\vec{x},t)}{\partial t} = R_s - \frac{k_{on}}{\epsilon} \cdot Ab(\vec{x},t) \cdot Ag(\vec{x},t) + k_{off} \cdot B(\vec{x},t) - k_e \cdot Ag(\vec{x},t)$$

$$\frac{\partial I(\vec{x},t)}{\partial t} = k_e \cdot B(\vec{x},t) - k_{resid} \cdot I(\vec{x},t)$$

 $Ab(\vec{x},t)$ = free antibody

 $B(\vec{x},t) = \text{bound antibody}$

 $Ag(\vec{x},t) = \text{antigen concentration}$

 $I(\vec{x},t) = \text{internalized}$

 k_{on} = antibody binding rate constant

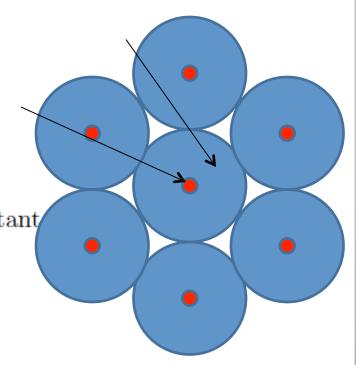
 k_{off} = antibody dissociation rate constant

 $\epsilon = \text{effective void fraction}$

 $k_e = \text{endocytosis}$ rate constant

 R_s = antigen synthesis rate

 k_{resid} = residualization rate constant



Mathematical modeling



Image Study Parameters			
Animal weight	Bo dy we ig ht	25 g (mouse)	
Activity	Injected activity	100-1000 uCi	Measure syringe activity before and after injection
Dose	Mass of compound injected	0.001-250 ug	Determine mass of injected compound (i.e. by absorbance)
Contrast Agent	R adiolabel/fluorophore	¹¹¹ In, ¹²⁵ I, ^{99m} Tc, etc.	,
Tumorsize	Mass of tum or	0.1-1 g	CT
Α	Fraction of alpha phase blood clearance	0.5-0.9	Blood activity over time or ELISA
t _{1/2, alpha}	Half-life of alpha phase blood clearance	1-12 h	Blood activity over time or ELISA
t _{1/2,beta}	Half-life of beta phase blood clearance	3-48 h	Blood activity over time or ELISA

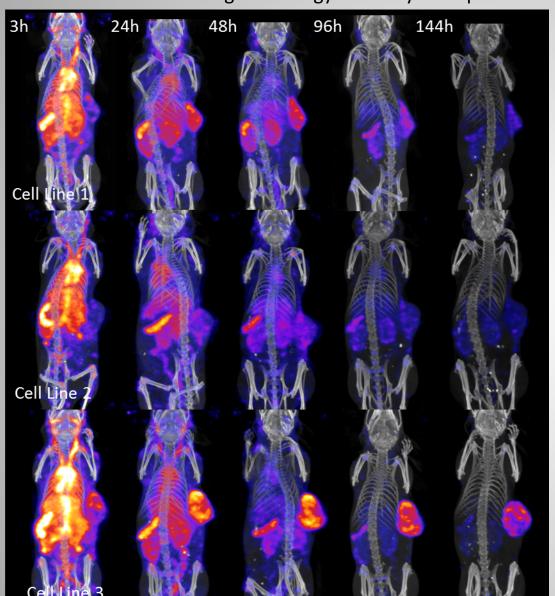
Mathematical modeling



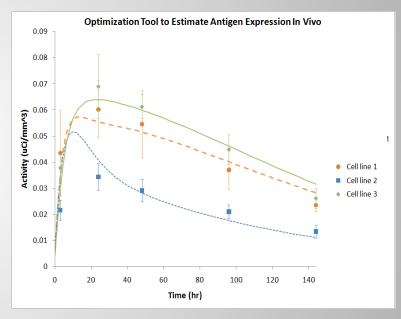
Parameter Inputs to Model

Parameter	Description	Typical Range	Assay
Ligand/Target Parameters			
K_D	Affinity	0.1 – 10 nM	Competitive cell binding (with radiolabeled or fluorescent compound)
MW	Molecular Weight	150 kDa (m Ab)	
t _{1/2,k e}	Half-life of cellular internalization	3-15 hours	Cell uptake over time (with radiolabled or fluorescent compound)
B_{max}	Antigen surface density	10 ³ -10 ⁶ #/cell	Competitive cell binding (with radiolabled compour or fluorescent compound with known standard)
ρ _{œll}	Cell density	10 ⁸ -10 ⁹ cells/mL	Ex vivo counting of Hoechst-stained nuclei in a known volume of tis sue
R	Half-distance from capillary to capillary (measure of vascularity)	20 – 150 μm	Ex vivo immunohistochemistry with CD31 staining
t _{1/2,kr s id}	Residualization rate	12-120 hours	Release of internalized compound over time (with radiolabeled compound)

Mathematical modeling – oncology antibody example.







Estimation of B_{max} and vascularity in three different tumor lines.

Other Considerations

Effect of molecular size – small and large are better than "medium".

Radiolabeling and ligand binding/function

Assay of cold-labeled materials

Clinical Translation

 How does the isotope/radioactive dose selection affect translatability

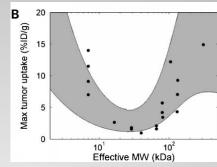
Specific activity and mass dose

- Does ligand bind? Is drug accumulation saturable?
- Does ligand exhibit off-target binding?
- How do metabolism/clearance/tissue distribution change with dose?
- Dose escalation studies are critical

Scaffold selection

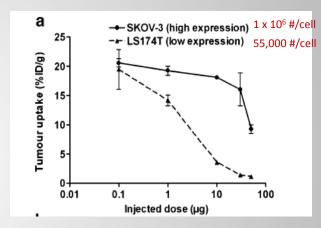
bsAb, IgG, minibody, diabody, scFv, affibody, peptide

Internalization Rates

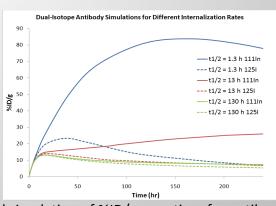




HER2 binding agents, Schmidt and Wittrup, 2009.



111In-labeled anti-HER2 affibody, Tolmachev et al. 2011



Model simulation of %ID/g over time for antibodies with different internalization rates (In111, I125)

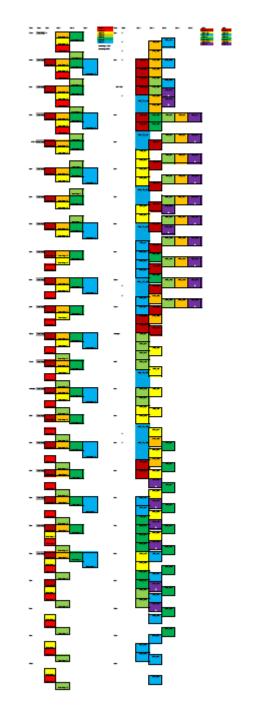
Study Management

Managing time.

- 274 SPECT/CTs over 7.5 days of around-clock-imaging
- Two injections of ~700-800uCi of I125-labeled antibody at 0 and again 74 or 97 hrs.
- Ab1: 1, 8.5, 16, 24, 36, 48, 75, 78.33, 81.67, 85, 91.67, 98.33, 110, 134
- Ab2: 1, 8.5, 16, 24, 36, 48, 72, 98, 105.5, 113, 121, 133, 145, 169
- 16 scientists/technical people

- Tumor growth
- Radioactive decay
- Scanner time
- Personnel hours
- Compound stability





Study Management

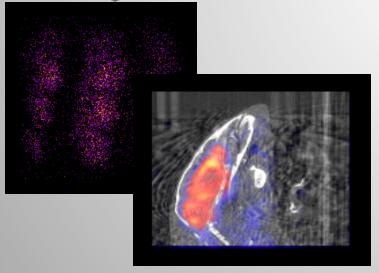
Managing time and distance.

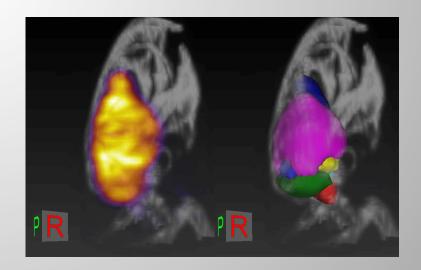




- Tumor growth
- Radioactive decay
- Scanner time
- Personnel hours
- Compound stability







Data Formats



Example Clinical Systems

GE Symbia GE Discovery **GE Biograph** Mediso AnyScan Philips Ingenia Philips BrightView Philips GEMINI **Siemens Discovery** Siemens Definition Siemens Magnetum

Example Preclinical Systems

ASPECT MR Bioscan NanoSPECT Bruker MR Caliper IVIS Optical **GE Locus** Mediso NanoScan Milabs uSPECT ScanCo CT Siemens Inveon SkyScan CT Varian MR

Clinical Data

DICOM

Preclinical Data

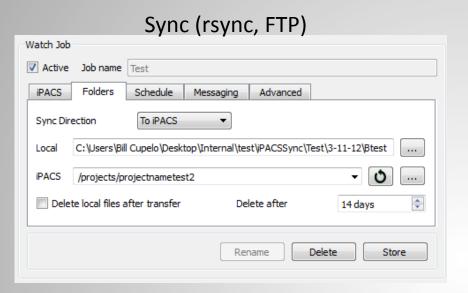
AIM **AVW BRUKER** DICOM IMG/HDR MHD/MHA NIFTI **RAW**

TIFF

DICOM data are standard, but many other formats require support.

Gathering the data





Drag-and-Drop (HTTP(S), Browser) Upload files for Christian Lackas Please select one or multiple files from your local computer to be uploaded to this iPACS system, then submit the form to complete the procedure. Do not leave this page until you are notified that the process was completed. Otherwise your data might get lost. — Upload a file Your name lacob (required) Company (optional) Your mail confirmation Files (one Upload files required) Comment (optional) Submit

The user is notified by mail once your file has been uploaded successfuly

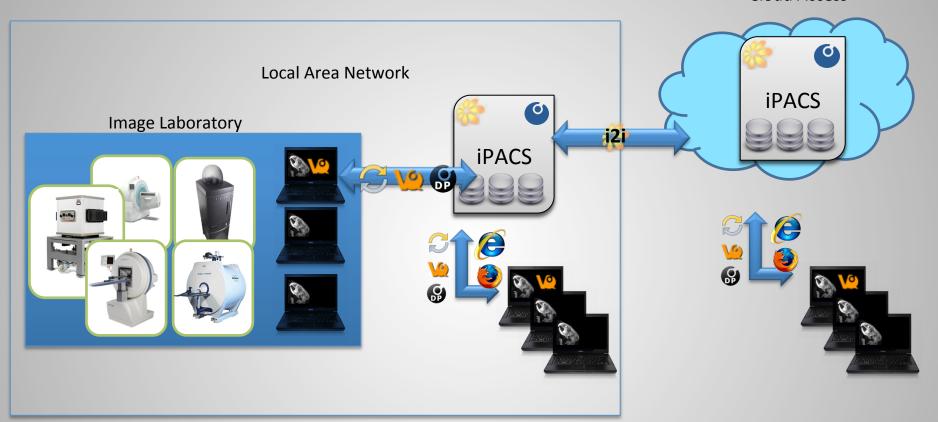
Direct DICOM transfer Study Browser Repository - SECURE Patients Name StudyDate StudyDescription iPACS Demo 2010-03-24 16:50 demoData1 DemoStudy demoData2 2010-03-26 17:40 DemoStudy /demoaccount1/tumortool 2010-03-08 17:09 DemoStudy Open data 2010-03-08 17:51 DemoStudy demoaccount1 Append data 2010-03-26 16:52 DemoStudy 2010-03-24 17:44 ▶ demo DemoStudy Projects: 7/215 Export to... 🧂 Local folder... Open in... 🎵 TempFolder Dump header PACS A iPACS CRO 🗶 Delete Data PACS E Patients Name: iPACS M Patient ID: iPACS inviCRO

Data transfer/upload options: DropBox, syncplicity, Cubby, huddle, ShareFile, iPACS

Image Analysis Gathering the data



Cloud Access





iPACS Sync: Keep local and remote folders in sync, secure transfer, optimized for large data sets



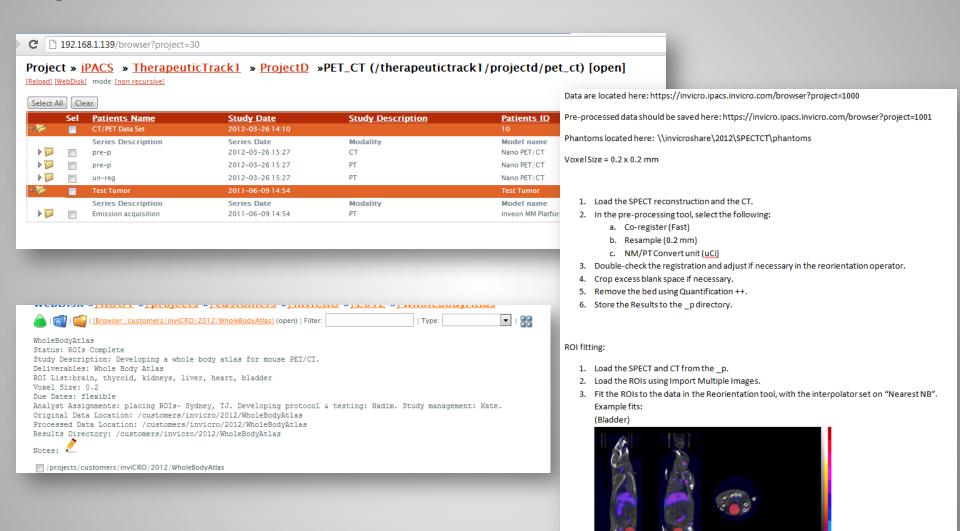
VivoQuant/InVivoScope provides full access to all iPACS data, integrated workflows



DICOM Proxy: Connect any DICOM client to the iPACS, e.g. DICOM export of imaging equipment, DICOM viewer, etc...

Organization

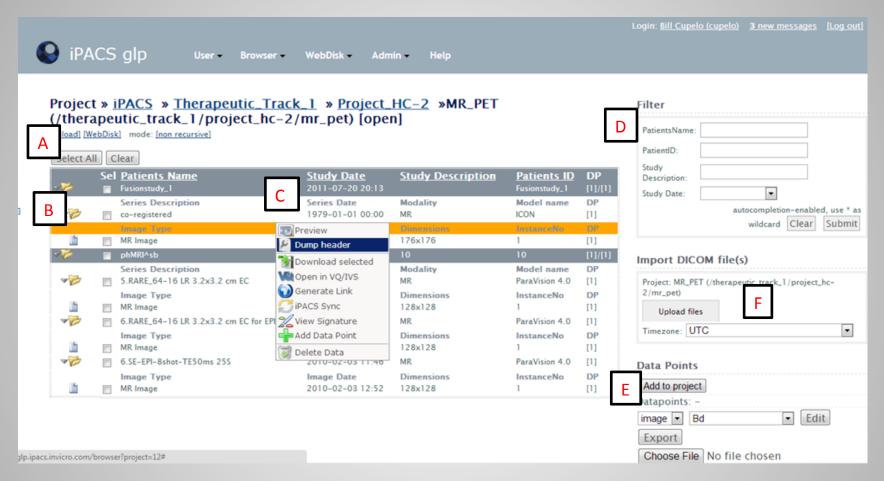




Define roles, deliverables, timelines, basic information for each study.

Gathering and indexing the metadata



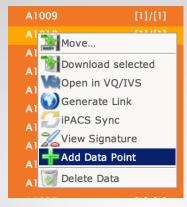


- A. Quickly switch between Browser and WebDisk view of a project, and move within project tree
- B. The iPACS Browser follows the DICOM standard hierarchy (Patient/Study/Series/Image).
- C. Download image data and/or open directly in the VivoQuant[™] desktop client.
- D. Filter over metadata fields.
- E. View data points associated with an individual image (e.g. Injected Dose, Cohort/Group Name, Weight, etc.).
- F. Upload DICOM files to current project via web, or use StoreSCU from your DICOM client

Example: Standard metadata

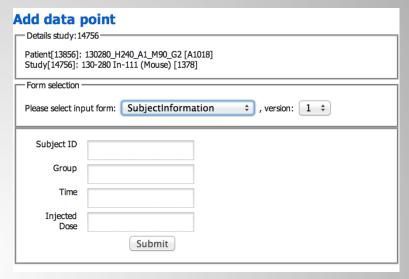






At different levels

ı	2012-03-01	cupelo	StudyUnits: 1	injdoseunit=uCi
ı	20:49			outputunit=uCi
ı				submit=Submit
ı				timeunit=d

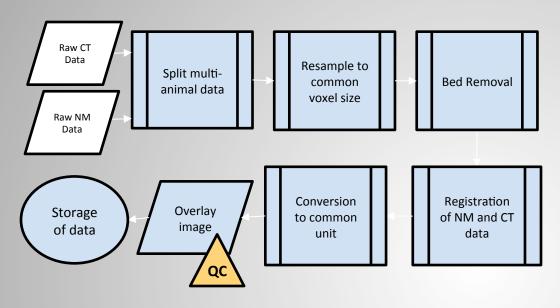


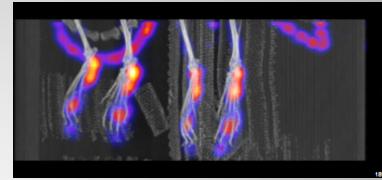
In Batch			Subject ID	Group	Timepoint	Injected Dose
130280_H0_A4_M13_G2 (A1018) 2012-08-14T18:44:16	NM	Whole Body SPECT (2) HiSPECT Reconstrution [Co-Reg] 2012-08-14T21:31:45 195043.532	1018	2	0.5	1354.53223991579
130280_H0_A4_M13_G2 (A1018) 2012-08-14T18:44:16	NM	Whole Body SPECT (3) HiSPECT Reconstrution [Co-Reg] 2012-08-14T21:31:48 200844.918	1018	2	0.75	1350.34337517629
130280_H0_A4_M13_G2 (A1018) 2012-08-14T18:44:16	NM	Whole Body SPECT (4) HiSPECT Reconstrution [Co-Reg] 2012-08-14T21:31:51 202646.405	1018	2	1	1346.1636073976
130280_H0_A4_M13_G2 (A1018) 2012-08-14T18:44:16	NM	Whole Body SPECT HiSPECT Reconstrution [Co-Reg] 2012-08-14T21:31:38 193224.241	1018	2	0.25	1358.80417523604

All SPECT (and PET) studies require knowledge of subject ID, group, timepoint, and injected dose.

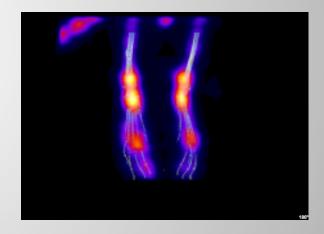
Preprocessing Image Data







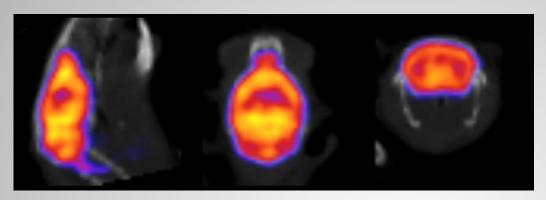


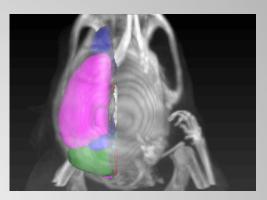


Critical components include:
Units
Documentation

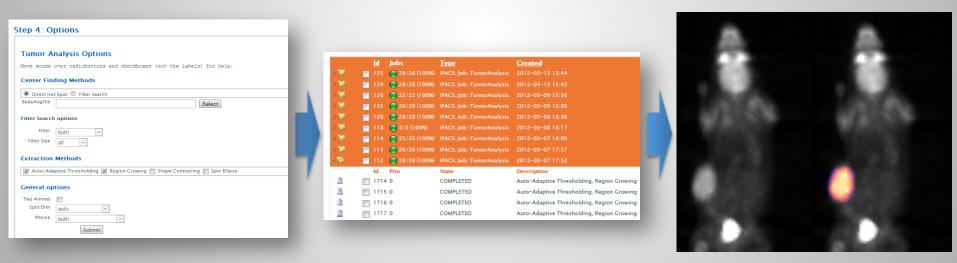
Extracting image information







Analysis of radiotracer distribution in the brain

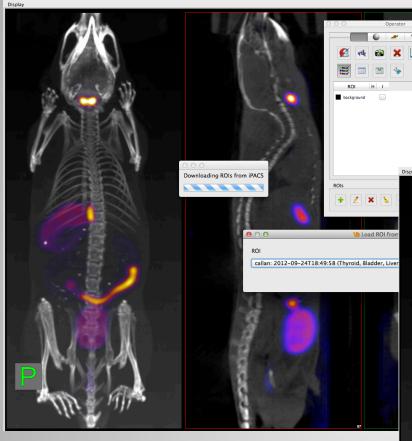


Analysis of radiotracer distribution in xenograft tumors.

Automation, and particularly semi-automation, are capable of reducing observer variability and speeding analysis times, but generalized tools are often time-consuming and expensive to develop.

Extracting Image Information



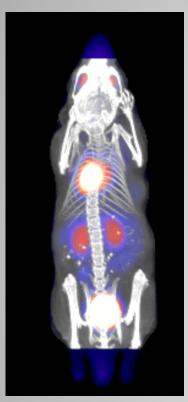


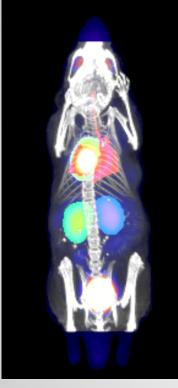
Standardizing protocols, improving low-level functionality, and removing inefficiencies can be more time-effective and beneficial than "magic segmentation buttons".



Storing Extracted Image Information







Critical components include:
Quality Control
Manual Intervention
Documentation
Standardization

	Sel	Patients Name	Study Date	Study Description	Patients ID	DP	
▼		M1	2012-06-28 20:16	Training		-/[1]	
		Series Description	Series Date	Modality	Model name	DP	
▶		Training	2012-06-28 21:06	CT	ModelName	[1]	
V		Training	2012-06-28 21:06	NM	ModelName	[1]	
		Image Type	Image Date	Dimensions	InstanceNo	DP	
		NM Reconstruction	2012-06-28 21:09	142x142	1	[15]	

Hierarchy: »series:46173 »studies:15083 »patients:13973 »projects:642 »projects:641 »projects:640 »projects:90 »projects:1 | Include parent points Data: Timestamp Creator Form Data Command 2012-09-24 16:02 tliguori | quantification:2 center=[67 109 134] color=darkred filename=/projects/customers/inviCRO/2012/WholeBodyAtlas/roi/roi-tliguori-M12-1348502471.rmha max=0.000149351 mean=0.000108765 min=8.27276e-05 2570769 name=Thyroid setid={7944c342-7639-42ec-93ce-eab7d0e02056} stddev=1.33151e-05 sum=0.130736

filename=/projects/customers/inviCRO/2012/WholeBodyAtlas/roi/roi-tliguori-M12-1348502471.rmha

unit=µCi volume=9.616 voxels=1202

color=yellow concentration=0.0244056

max=0.000288118 mean=0.000195245

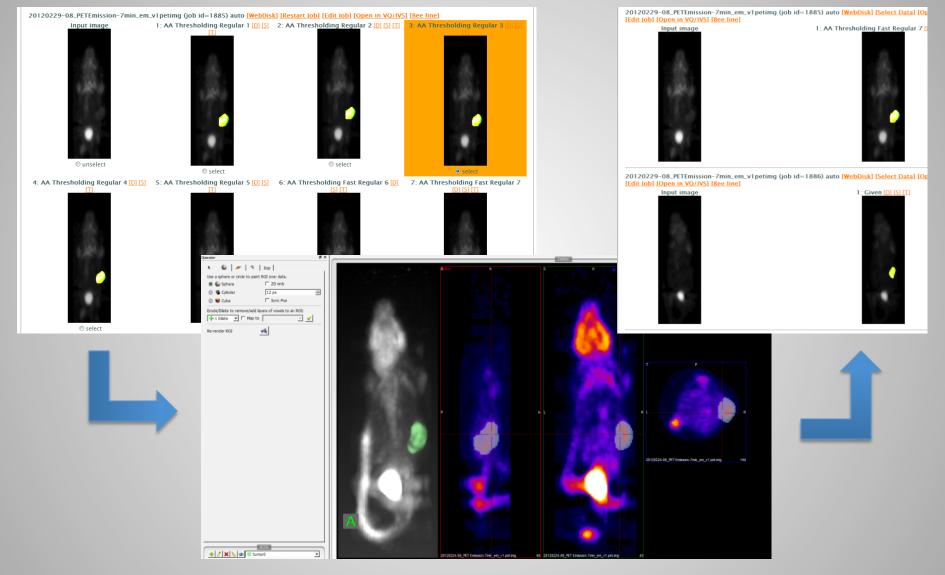
2012-09-24 16:02 tliguori | quantification:2 center=[63 100 364]

Data points for Image[972932]: ORIGINAL\PRIMARY\RECON TOMO\EMISSION []

8 datapoints found

Editing and Reviewing Regions of Interest

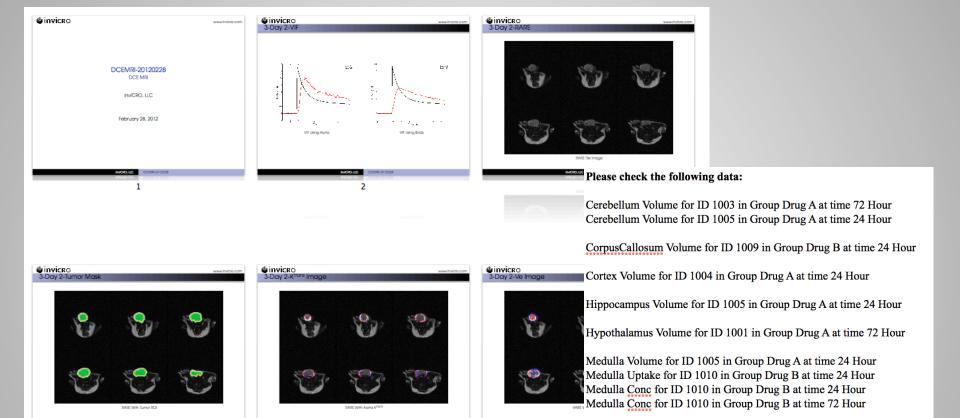




Example: Individual tumors are QC'd, manually edited in VQ, and re-run as necessary.

Quality Control Records – Qualitative and Quantitative





Pons Volume for ID 1008 in Group Ctl A at time 72 Hour Pons Uptake for ID 1010 in Group Drug B at time 24 Hour Pons Conc for ID 1010 in Group Drug B at time 24 Hour

Midbrain Volume for ID 1008 in Group Ctl A at time 24 Hour

Olfactory Volume for ID 1003 in Group Drug A at time 72 Hour Olfactory Volume for ID 1005 in Group Drug A at time 24 Hour

Quality control of registrations, estimates, segmentations, etc. are essential.

Extracting image information





Scripting is a powerful tool for accessing image data, image processing, generation of quality control images and spreadsheets.

Master Spreadsheet and Plotting Tool

```
GINVICRO imaging services and software
```

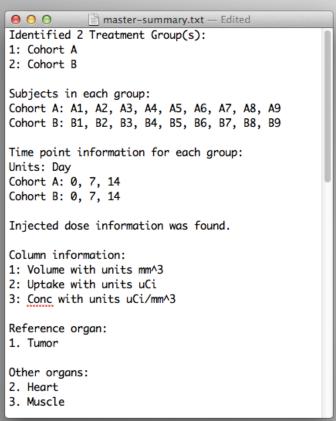
```
%- prj = Model.table('projects').find(planid);
   UNLESS formname.defined; formname = 'quantification'; END;
   UNLESS level.defined; level = 'images'; END;
   UNLESS organs.size;
     organs = prj.findUniqueDPValues('name', formname, level, 1);
    END;
   UNLESS isotope.defined; isotope = '.?'; END;
   UNLESS modality.defined; modality = 'NM'; END;
   unitInfo = prj.lastDataPointsByForm_rs('StudyUnits');
    CSV.push('iPACS Master Spreadsheet');
   CSV.push('Project', prj.toString, '', 'Modality', modality);
    CSV.add('Subject ID','Group',
            'Time (' _ unitInfo.value('timeunit') _ ')',
           'Injected Dose (' _ unitInfo.value('injdoseunit') _ ')');
   IF metadata.size; CSV.add(metadata); END; # Add extra metadata column headers
    CSV.add('SeriesDesc');
```

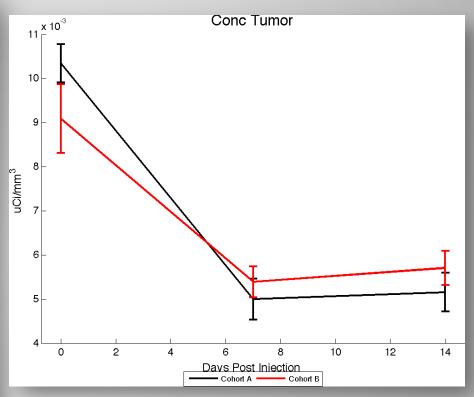
Subject ID	Group	Time (d)	Inj Dose (uCi)	Tumor Volume (mm^3)	Tumor Uptake (uCi)	Tumor Conc (uCi/mm^3)	Tumor Percent ID (% ID)	Tumor Percent ID/g (%ID/g)
A1	Cohort A	0	206.065	130.792	1.47264	0.0112594	0.714648	5.464
A2	Cohort A	0	210.739	201.368	2.11727	0.0105144	1.00469	4.98932
A3	Cohort A	0	209.5	196.288	2.22335	0.011327	1.06126	5.40667
A4	Cohort A	0	180.346	151.648	1.31912	0.00869853	0.731439	4.82327
A5	Cohort A	0	195.196	180.984	1.91043	0.0105558	0.978722	5.40778
A6	Cohort A	0	184.387	162.192	1.5087	0.00930197	0.818223	5.04478
A7	Cohort A	0	211.943	104.664	1.25813	0.0120206	0.593617	5.67165
A8	Cohort A	0	211.09	138.304	1.1372	0.00822248	0.538727	3.89524
A9	Cohort A	0	197.547	135.36	1.5127	0.0111754	0.765743	5.65708
B1	Cohort B	0	207.49	174.736	2.4013	0.0137424	1.15731	6.62318
B2	Cohort B	0	202.777	293.768	2.48691	0.00846555	1.22643	4.17481
B3	Cohort B	0	220.63	194.784	2.00484	0.0102926	0.908688	4.6651
B4	Cohort B	0	178.072	305.536	1.80093	0.00589435	1.01135	3.31008
B5	Cohort B	0	183.821	176.824	1.58014	0.00893621	0.85961	4.86139
B6	Cohort B	0	210.654	195.184	1.97782	0.0101331	0.938897	4.81032
B7	Cohort B	0	209.055	174.792	1.77007	0.0101267	0.846701	4.84405
B8	Cohort B	0	206.634	184.816	1.36791	0.00740149	0.661996	3.58192
B9	Cohort B	0	207.759	236.504	1.61074	0.00681063	0.775294	3.27814
A1	Cohort A	7	202.265	477.776	1.81976	0.00380882	0.899689	1.88308
A2	Cohort A	7	207.542	1136.36	3.08062	0.00271096	1.48434	1.30622
A3	Cohort A	7	193.35	614.44	3.82172	0.00621984	1.97658	3.21688
A4	Cohort A	7	203.159	279.192	1.55026	0.00555267	0.763079	2.73317

Scripts may be run on the iPACS, in VQ, or locally (using iPACS APIs) to access image information.

Master Spreadsheet and Plotting Tool





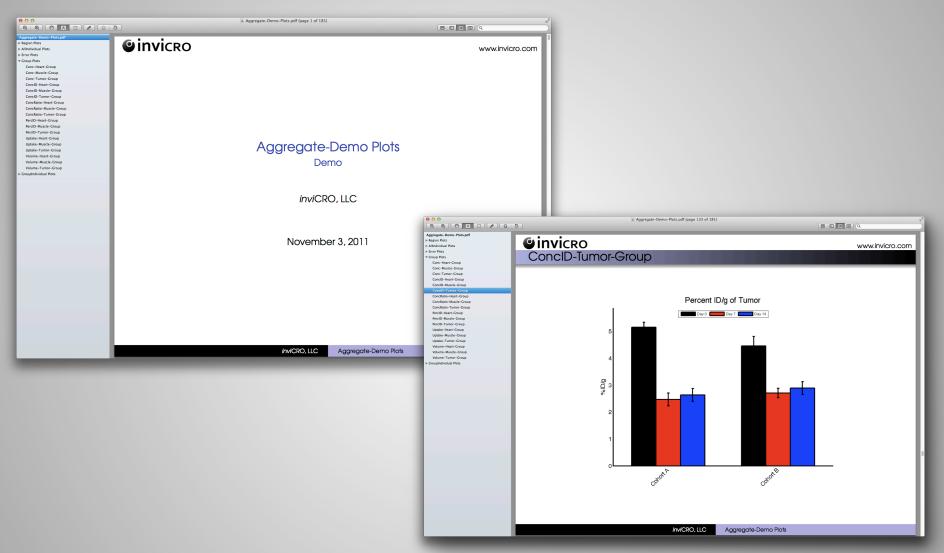


Quantity	Organ	Group	Sample 1	Sample 2	Paired t-test	P-Value	Result	Comment
Volume	Tumor	All Subjects	Day 0	Day 7	Two-tailed	6.77E-08	Mean B > Mean A	VHS
Volume	Tumor	All Subjects	Day 0	Day 14	Two-tailed	1.57E-06	Mean B > Mean A	VHS
Volume	Tumor	All Subjects	Day 7	Day 14	Two-tailed	0.0115557	Mean B > Mean A	S

The plotting tool accepts a settings file and the master spreadsheet to generate output materials, including plots, a summary, output spreadsheets, and hypothesis testing results.

Master Spreadsheet and Plotting Tool

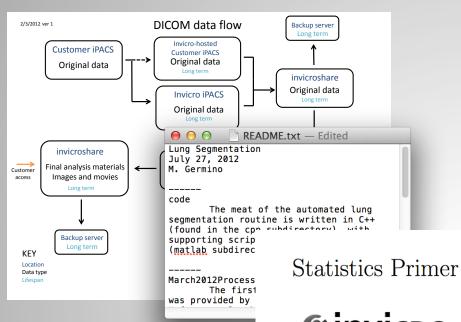




The plotting tool accepts a settings file and the master spreadsheet to generate output materials, including plots, a summary, output spreadsheets, and hypothesis testing results.

Reporting





Maintaining SOPs and internal documentation.

invicro

Au THE INVICRO COMPREHENSIVE GUIDE TO IMAGE AND MOVIE GENERATION

Critical components include: **Present Succinctly** Maintain Internal Documentation **Standardize Output Structures** Make Everything Available

INVICRO, LLC

PART 0: Overview of Image and Movie Generation Tools 3 PART 0: Overview of Image and Movie Generation Tools

Introduction PART I: Classification of Images and Movies

CT/NM MIPs NM/ROI MIPs Calculating nanoMolar Quantification Factor

Kevin Magalhaes inviCRO, LLC

July 9, 2012

Image Analysis Reporting

MRI Functional Connectivity inviCRO, LLC. MRI Functional Connectivity inviCRO, LLC.

3.2.2 Functional Connectivity Analysis

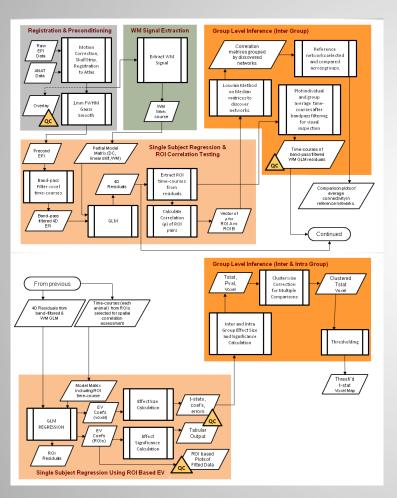


Figure 3: Pipeline for Functional Connectivity Analysis

CONFIDENTIAL 12 July 3, 2012



6 SUPPLEMENTAL

Often, output materials are generated in preparation or during an imaging study. For reference, links to many of these materials are provided here, with a brief description.

Functional connectivity analysis raw materials for subject level analysis using bandpass filter of 0.001Hz to 0.01Hz: Subject output for alternate BPF window

Slides from early considerations of design matrix setup, including use of a longer ideal ramp function for phMRI analysis and example signal fits: Slide Deck 1

Slides from initial examination of effect from cluster-wise correction for multiple comparisons: Slide Deck 2

Slides from initial work on correlation matrix functional connectivity analysis using paired tests: Slide Deck 3

Slides from initial work on GLM based functional connectivity analysis without White Matter regression pre-processing: Slide Deck 4

Slides from initial work testing the effects of bandpass filtering on functional connectivity analysis: Slide Deck 5

Slides comparing results using different registration and slice selection methods for spatial normalization and group analysis: Slide Deck 6

Slides comparing results using the different registrations mentioned above, but with maps that are uncorrected for multiple comparisons. Slide Deck 7

Slides from initial results of phMRI analysis results including workflow at that stage of analysis: Slide Deck 8

Slides comparing results from using White Matter and White Matter plus CSF region signals as nuisance regressors: Slide Deck 9

Slides with initial proposal of phMRI and functional connectivity analysis workflows: Slide Deck 10

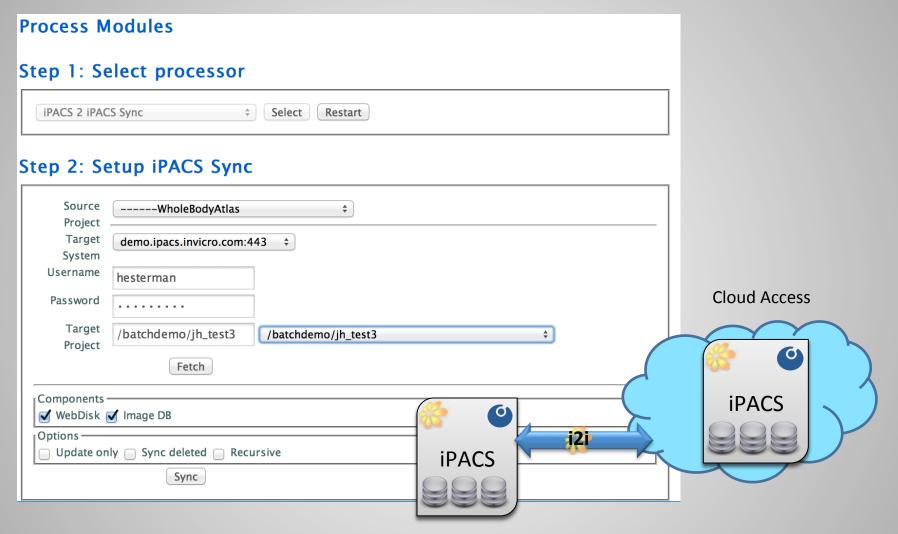
Slides for results prior to fixing degrees of freedom issue in group analyses.

- phMRI Results: Slide Deck 11
- Un-thresholded Functional Connectivity Results: Slide Deck 12
- MC-Corrected Functional Connectivity Results: Slide Deck 13

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Reporting





Disseminating results entails similar challenges to gathering of data. Methods are required that enable transfer of processed data, metadata, and results (reports, plots, etc.).



Design, Management, Analysis, Reporting

- Careful planning, including selection of isotope, animal number and kind, mass dose, and radiochemistry strategy are required.
- A variety of pre-imaging assays (i.e., dose escalation studies) can greatly aid the success of the final imaging study.
- Multiple moving, time-sensitive parts require coordination so logistics are critical.
- Clearly defined roles & responsibilities and teamwork are essential to hitting imaging time points successfully.
- Data analyses starts (flow of data from acquisition site to analysis platform) and ends (flow of data from analysis/reporting platform to sponsor) with data management.
- Reproducibility, efficiency, and attention to detail (i.e., units, documented and reproducible computation) are all critical.
- Storage of data and metadata in a generalized, script-accessible, well-documented format important for long-term access and analysis.

Summary

Other Considerations



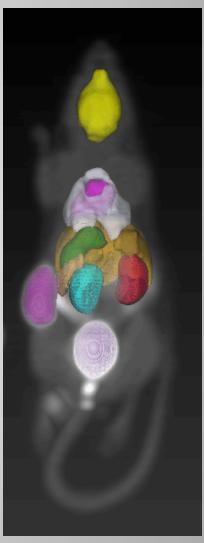
- PK modeling and sub-organ analyses are critical unique features of preclinical in vivo imaging.
- Imaging is expensive but contains a wealth of information – more (i.e., data mining, increased standardization of acquisition/reconstruction protocols) is required to make it possible for image information to be shared across studies.
- The use of MR and optical imaging in conjunction with NM imaging is of growing importance.
- The right applications should be targeted for in vivo imaging studies.

Thursday, 1:30-2:30PM Session

Title: Pre-clinical SPECT/CT-Specific Applications and Case Studies

The content will be case studies, particularly with respect to why we use SPECT/CT in translational research.





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inviCRO, LLC

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Nadim Farhat, MSc

Balázs Viszoczki, MSc Kate Sokolnicki, BS Mary Germino, BS Catey Harwell, BS Stefanie Feldmann, MA Deirdre Scully, BS Rob Callan, BS Jaime Tierney, BS Edwin Crockford, MA Justin Loutsch, BS Kevin Magalhaes Whitney Woodson, MSc

Consultants: Ed Soares, PhD Steve Mather, PhD Nils Schramm, PhD